

# **Nonlinear Lateral Interactions in V1 Population Responses Explained by a Contrast Gain Control Model**

Abbreviated Title: V1 Population Responses Explained by Gain Control Model

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## Abstract

How do cortical responses to local image elements combine to form a spatial pattern of population activity in primate V1? Here we used voltage-sensitive-dye imaging (VSDI), which measures summed membrane potential activity, to examine the rules that govern lateral interactions between the representations of two small local oriented elements in macaque (*Macaca mulatta*) V1. We find strong sub-additive and largely orientation-independent interactions for nearby elements (2-4mm inter-element cortical distance; IED) that gradually become linear at larger separations ( $> 6$ mm IED). These results are consistent with a population gain control model describing nonlinear V1 population responses to single oriented elements. However, due to the membrane-potential-to-spiking accelerating nonlinearity, the model predicts supra-additive lateral interactions of spiking responses for intermediate separations at a range of locations between the two elements, consistent with some prior facilitatory effects observed in electrophysiology and psychophysics. Overall, our results suggest that population-level lateral interactions in V1 are largely explained by a simple orientation-independent contrast gain control mechanism.

## Significance Statement

Interactions between representations of simple visual elements such as oriented edges in primary visual cortex (V1) are thought to contribute to our ability to easily integrate contours and segment surfaces, but the mechanisms that govern these interactions are largely unknown. Our study provides novel evidence that lateral interactions at the population level are governed by a simple contrast gain-control mechanism, and we show how this divisive gain-control mechanism can give rise to apparently facilitatory spiking responses.

## Introduction

Primary visual cortex (V1) is organized topographically; neurons with similar tuning properties cluster together, forming several overlaid maps across the cortical surface. At the large (millimeter) scale, V1 contains a map of position in visual space (retinotopic map) (Hubel and Wiesel, 1974; Van Essen et al., 1984; Tootell et al., 1988; Adams and Horton, 2003). Because the tuning properties of neighboring V1 neurons overlap extensively, a small isolated stimulus produces activity spreading over several square millimeters (Hubel and Wiesel, 1974; Van Essen et al., 1984; Grinvald et al., 1994). This spread (termed the cortical point image; CPI) has a full-width (at 10% of the peak response) of up to 8 mm for membrane potential and up to 4 mm for spiking activity (Palmer et al., 2012). Natural scenes usually contain many elements at nearby spatial locations. Thus, when viewing natural scenes, V1 responses to the component elements overlap substantially. This raises a fundamental question: How do cortical responses to local image elements combine to form the spatial pattern of population activity in primate V1?

In previous studies using VSDI we measured V1 population responses to single oriented elements (Sit, Chen et al. 2009). We discovered that V1 responses to single elements are predicted by a simple computational model, termed “population gain control” (PGC). Our goal here was to determine whether this model also predicts V1 population responses to multiple local elements. Specifically, the PGC model assumes that local gain is controlled by a normalization pool that is independent of the orientation and direction of a flanking element relative to a central element, but this assumption has not been fully tested. For example, it is possible that flanking elements collinear or parallel with a central element make a larger contribution to the normalization pool, thereby leading to stronger sub-additivity than

equally-distance elements orthogonal to the central element. A central goal of the current study was to test this possibility.

While gain control mechanisms may explain some interactions in V1, facilitatory mechanisms may also be at play. Perception of a visual element can be profoundly modulated by nearby visual elements. Under some circumstances, detection of a small contour element is facilitated by nearby flanking elements (Polat and Sagi, 1993, 1994). Similarly, there is behavioral evidence of grouping mechanisms that integrate local contour elements into extended contours (Field et al., 1993). The first stage of this process may involve local mechanisms that facilitate the representations of two visual elements if they are likely to belong to the same contour in natural scenes (Field et al., 1993). This facilitatory associative mechanism may be partially implemented in V1, and mediated by its long-range horizontal connections (Gilbert and Wiesel, 1979; Ts'o and Gilbert, 1988; Hirsch and Gilbert, 1991) and/or by feedback connections into V1 (Angelucci et al., 2002). Alternatively, facilitatory mechanisms underlying perceptual grouping may be implemented downstream of V1, and V1 retinotopic-scale interactions may be fully explained by the PGC model.

Studies of single V1 neurons reveal diverse effects of flanking stimuli on spiking responses to a central element. Some studies using large surround stimuli show clear suppression consistent with gain control mechanisms (e.g., Sceniak et al., 1999; Cavanaugh et al., 2002a; Levitt and Lund, 2002), while others show configuration-specific facilitation consistent with an associative grouping mechanism (e.g., Maffei and Fiorentini, 1977; Kapadia et al., 1995; Polat et al., 1998). Given the diversity of these effects, it is unclear how flanking stimuli will affect neural responses at the population level. While several previous optical imaging experiments demonstrate sub-additive lateral effects at the population level in V1 (Kinoshita et al., 2009; Meirovithz et al., 2010; Reynaud et al., 2012), it is possible that suppressive

effects dominate at the population level for some flanker positions and orientations while facilitatory effects dominate for others.

We addressed these questions using VSDI to measure population responses from V1 of three fixating monkeys while presenting individual and pairs of oriented elements.

## Materials and Methods

The results reported here are based on methods that have been described in detail previously (Chen et al., 2006, 2008). Here, we focus on details that are of specific relevance to the current study. All procedures have been approved by the University of Texas Institutional Animal Care and Use Committee and conform to NIH standards.

### ***Experimental Design and Statistical Analysis***

The experiments described below incorporated a within-subjects design, with different stimulus configurations presented in pseudorandom sequences of trials within individual experimental sessions. In characterizing our results, we do not use traditional null-hypothesis significance tests (NHSTs). Instead, we report point and interval estimates of the relevant response parameters (population response amplitudes and facilitation indices). Details of these analyses are described in the *Analysis of Imaging Data* section below and in the *Results* section.

### ***Behavioral Task and Stimuli***

Three male adult monkeys (*macaca mulatta*) were trained to maintain fixation while a small stationary Gabor or a combination of Gabors was presented on a uniform gray background. Each trial began when the monkey fixated on a small spot of light (0.1 deg) on a CRT display. Following an initial fixation, the

sine-phase Gabor stimuli ( $\sigma = 0.167^\circ$ ,  $f = 2\text{cpd}$ ) were flashed at 5Hz for 1000 ms (60ms on, 140ms off) at visual eccentricities between 2.40 and 3.82 degrees. Throughout the trial, the monkey was required to maintain gaze within a small window ( $<2\text{deg}$  full width) around the fixation point in order to obtain a reward. The contrast of the flanking stimulus element, when presented, was 100%, while the central stimulus element appeared at 10%, or 100% contrast. Stimuli were displayed at a mean luminance of 30  $\text{cd/m}^2$ , at a resolution of 1024 x 768 pixels (subtending  $20.5^\circ \times 15.4^\circ$  of visual angle), a viewing distance of 108 cm, a 30-bit color depth, and a refresh rate of 100 Hz. In each session, trials representing the different visual stimulus conditions, including blank trials, were randomly interleaved. On average, the monkeys successfully completed 10 trials per condition per session.

### ***Analysis of Imaging Data***

Imaging data were collected at 110Hz at a resolution of  $512 \times 512$  pixels. The size of each pixel was approximately  $32 \times 32 \mu\text{m}^2$ . Our basic analysis was divided into four steps. First, we normalized the responses at each pixel by the average fluorescence at that pixel across all trials and frames. Second, we removed from each pixel a linear trend estimated on the basis of the response in the 100 ms interval before stimulus onset for each trial. Third, we removed trials with aberrant VSDI responses (generally fewer than 1% of the trials). Finally, we subtracted the average response to the blank condition from the stimulus-present conditions. In a supplementary analysis not presented here, we checked for fixation effects by additionally removing trials in which the monkey's gaze deviated more than  $0.5^\circ$  from the fixation point. However, we found that this manipulation did not meaningfully affect our results.

After this analysis, the spatial properties of the responses in each trial were determined. To preserve our ability to characterize the amplitude of each response independently of its temporal properties (e.g., response onset and offset latency, rising edge slope, falling edge slope), we fit a parametric temporal

impulse response model to the response timecourse measured at each pixel. The temporal response to a single flashed stimulus  $r_{pulse}(t)$  is well described by a scaled gamma distribution function

$$r_{pulse}(t) = r_0 + A\gamma(t - t_0; \alpha, \beta), \quad (1)$$

where  $A$  is the response amplitude,  $t_0$  is the response onset latency,  $r_0$  is the baseline response, and  $\gamma(x; \alpha, \beta)$  represents the (unnormalized) gamma distribution function with shape parameter  $\alpha$ , rate parameter  $\beta$ , and a maximum value of 1.

$$\gamma(x; \alpha, \beta) = \begin{cases} \left(\frac{\beta x}{\alpha - 1}\right)^{\alpha - 1} e^{-\beta x - 1} & x \geq 0 \\ 0 & x < 0 \end{cases} \quad (2)$$

Measured responses to the five-pulse sequences were well fit by a model that used a common impulse function for each of the five flashes and combined the individual pulse responses using a max rule (see Figure 1c), such that

$$r(t) = \max \{r_{pulse}(t; A, t_0 + 0.2n, r_0, \alpha, \beta) \mid n = 0, 1, 2, 3, 4\}. \quad (3)$$

For each experiment, we computed the average spatial response amplitude  $\bar{A}$  at each pixel by fitting Eqn. (3) to the average time course at that pixel. We computed the variance of this estimate using a delete-1 jackknife procedure (Efron and Stein, 1981). For each condition, we estimated mean spatial amplitudes for  $n$  subsamples of the trials in which each sample was formed by omitting one of the observations. For example, the  $i^{\text{th}}$  mean was computed as

$$\bar{A}_i = \frac{1}{n-1} \sum_{j \neq i}^n A_j. \quad (4)$$

The jackknife estimate for the variance of the mean amplitude was then computed from these means as

$$\sigma_A^2 = \frac{n-1}{n} \sum_i^n (\bar{A}_i - \bar{A})^2. \quad (5)$$

## Computation of Pooled Responses

For the summary spatial response plots in Figures 4 and 5, we pooled the response amplitudes by computing a weighted average across all animals (N=3) and experiments (N=14; 5 for Monkey 1, 6 for Monkey 2, and 3 for Monkey 3). The weighting served two purposes. First, the experiments were of variable quality and we wanted to give greater weight to the more reliable experiments. Second, the cortical magnification factor (CMF) varied across monkeys and across stimulus locations, so that the cortical distance associated with a particular visual IED also varied across experiments. Because the size of the CPI is roughly constant across V1 (Palmer et al., 2012), we expected the interactions among visual elements to depend primarily on the cortical distance between their elicited responses (the cortical IED) rather than on their distance in visual coordinates (the visual IED). Our analyses therefore focused primarily on characterizing the interactions as a function of the cortical IED, which is equal to the separation in the visual field times the CMF. In computing the pooled responses, we assigned two weights to each experiment and condition, one ( $u$ ) representing the reliability of the amplitude estimate for that experiment, and one ( $w$ ) representing an interpolation weight for the desired cortical IED. The pooled response amplitude for a particular location  $x$  was computed as

$$A_p(x; \varepsilon) = \frac{1}{\sum_j^N u_j w_j(\varepsilon)} \sum_i^N u_i w_i(\varepsilon) A_i(x) \quad (6)$$



where  $\varepsilon$  represents the cortical IED for which we want to interpolate the responses and  $N$  is the combined number of different experiments and visual IED conditions. The reliability weights were computed as

$$u_i = \frac{1}{\sigma_{A_i}^2}, \quad (7)$$

where  $\sigma_{A_i}$  is the standard error associated with the amplitude estimate for experiment/condition  $i$ . This weight has the effect of reducing the contribution of variable (unreliable) experiments to the pooled amplitude estimate. The average value of these reliability weights varied across monkeys, with responses from Monkeys 2 (across 6 experiments) and 3 (across 3 experiments) receiving greater weight than those from Monkey 1 (across 5 experiments). As a result of the differing reliability weights and numbers of experiments, each monkey contributed differently to the pooled responses (Monkey 1: 23%, Monkey 2: 48%, Monkey 3: 29%). However, supplementary analyses (not shown) confirmed that response patterns did not differ meaningfully across individual monkeys.

The interpolation weights were Gaussian (i.e., a Gaussian radial basis function)

$$w_i(\varepsilon) = e^{-\frac{(\varepsilon_i - \varepsilon)^2}{2\sigma_{RBF}^2}}, \quad (8)$$

where  $\varepsilon_i$  represents the cortical IED for the  $i^{\text{th}}$  experiment/condition, and  $\sigma_{RBF} = 1$  mm is the standard deviation of the radial basis function. This weight has the effect of attenuating the contributions of experiments/conditions as their cortical IEDs deviate from the desired cortical IED  $\varepsilon$ . We computed variances for the pooled amplitude estimates by linearly combining the jackknife variance estimates

from individual experiments obtained into Eqn. (5) using weights identical to those in Eqn. (6), which we then used to compute the symmetric 95% confidence bounds shown in Figures 4, 5a, and 5b.

Finally, we found that the resulting spatial responses had a small positive baseline response equal on average to approximately 8% of the maximum response. We removed this baseline when plotting the summary responses (Figures 4 & 5) and when computing the corresponding facilitation indices. This had the effect of raising the facilitation indices slightly, making the combined responses appear somewhat less subadditive than when the baseline was included.

### **Computing Pooled Facilitation Indices**

Average facilitation indices were computed by applying Eqn. (12) to the pooled population response amplitudes. We obtained interval estimates around the average values using a simple parametric bootstrap procedure (Efron, 1985). For each stimulus configuration, we created 10,000 bootstrap replicates of the spatial response to the central, flanker, and combined stimuli by sampling from normal distributions with average amplitudes and variances computed as described in *Computation of Pooled Responses*. We then computed a distribution of facilitation indices by applying Eqn. (12) to each of the bootstrapped replicates. Finally, we obtained 95% confidence intervals by determining the facilitation indices corresponding to the 2.5<sup>th</sup> and 97.5<sup>th</sup> percentiles of this distribution.

### ***PGC Model Definition and Simulation***

The structure of the population gain control model is identical to that defined in Sit et al. (2009). Briefly, the model consists of an input layer representing the raw visual input, a second layer representing the local spatial summation and gain control arising in the retina, LGN, and the input layers of V1, and a third layer that represents the local spatial summation and gain control in the superficial layers of V1,

where the VSDI responses are measured. Each unit in the second and third layers computes the weighted sum of the input  $I(x, t)$  by cross-correlation with a Gaussian spatial receptive field:

$$A(x, t) = I(x, t) \star G(x), \quad (9)$$

where  $G(x)$  is a zero-centered Gaussian function with standard deviation of  $\sigma_G$ . The summation then passes through an RC circuit to produce the response, which is characterized by the differential equation

$$C \frac{dV(x, t)}{dt} = A(x, t) - g(x, t)V(x, t), \quad (10)$$

where  $C$  is the capacitance,  $A(x, t)$  is the receptive field summation activity and  $g(x, t)$  is the conductance of the resistor for the stage. The conductance at each unit is defined as

$$g(x, t) = 1 + bI(x, t) \star H(x) \quad (11)$$

where  $b$  is a scaling factor that represents the strength of normalization and  $H(x)$  is the Gaussian weighting function (with standard deviation  $\sigma_H$ ) defining the normalization pool.

The parameters for all units within the same layer are identical, but they can differ between stages. Additionally, because the response in each model stage represents average membrane potentials, responses in the first stage are converted to spikes by a power function before being sent to the second stage.

The PGC model is characterized by a total of 9 parameters. Four parameters ( $\sigma_{G_1}, \sigma_{H_1}, C_1, b_1$ ) characterize the first response layer, another four parameters ( $\sigma_{G_2}, \sigma_{H_2}, C_2, b_2$ ) characterize the second response layer, and one parameter ( $n$ ) represents the spiking nonlinearity. In simulating the PGC model,

we fixed the values of 4 of these parameters ( $C_1, C_2, b_2$ , and  $n$ ) to those used by Sit et al. (2009). In addition, like Sit et al. (2009), we assumed that the receptive and normalization fields in the second response layer were twice the size of those in the first input layer (i.e.,  $\sigma_{G_2} = 2\sigma_{G_1}$  and  $\sigma_{H_2} = 2\sigma_{H_1}$ ). This left us with three free parameters: the sizes of the receptive ( $\sigma_{G_1}$ ) and normalization ( $\sigma_{H_1}$ ) fields in the first input layer and the strength ( $b_1$ ) of the normalization in the first layer. We estimated the values of these parameters by adjusting them such that (1) the normalized response to the 10% center stimulus matched that obtained for the pooled VSDI responses, (2) the width of the PGC responses matched the width of the pooled VSDI responses, and (3) the facilitation index obtained for the PGC responses (Figure 6D) approximately matched that obtained for the VSDI responses in the 1° IED condition (Figure 4; top right). The obtained parameters were  $\sigma_{G_1} = 0.87$  mm,  $\sigma_{H_1} = 1.07$  mm, and  $b_1 = 500$ . The model was simulated for a 20mm long strip centered on the response to the center element.

## Results

We used VSDI to measure population responses to briefly flashed individual or pairs of spatial Gabor stimuli (sine phase, spatial frequency = 2 cpd,  $\sigma = 0.167^\circ$ ) in the primary visual cortex of three male macaque monkeys performing a fixation task.

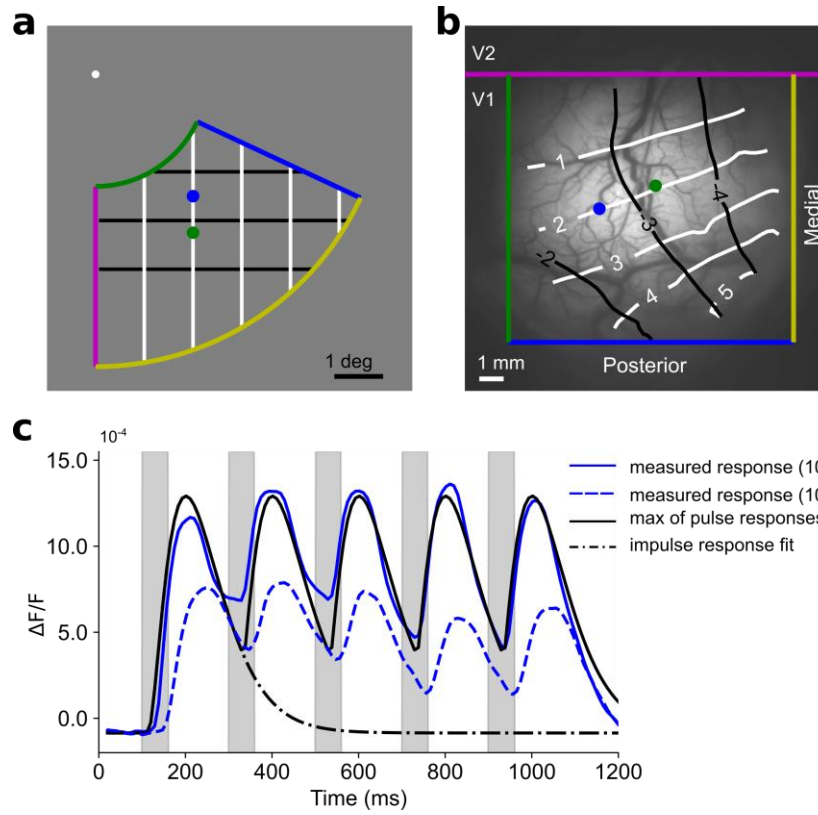
Two features of our measurements are important to consider. First, VSDI signals are directly proportional to membrane voltage and reflect aggregate synaptic inputs to neurons in layers 1-3. We consider the potential implications of our results for understanding lateral interaction at the level of the spiking output in the discussion section. Second, while VSDI in behaving monkeys can measure reliable signals at the columnar scale ( $\sim 1.2$  cyc/mm; Chen et al., 2012), such high-resolution imaging requires

240 zooming in on a small cortical area. Here, instead, we focus on maximal coverage, which is necessary in  
241 order to image the entire retinotopic-scale population response to local elements (the subthreshold CPI).  
242 The nature of lateral interactions at the orientation columns scale will be examined in future studies. Our  
243 previous VSDI studies in behaving monkeys have demonstrated that retinotopic-scale V1 signals contain  
244 enough information to account for detection performance (Chen et al., 2006, 2008) and may contribute  
245 to shape perception (Michel et al., 2013). Therefore, it is important to characterize the nature of lateral  
246 interactions in V1 at this fundamental scale.

247 In preliminary measurements, we used a mapping procedure (Yang et al., 2007) to determine the precise  
248 layout of the retinotopic map in the imaged area (Figures 1a-b). We then positioned the Gabor stimuli  
249 such that the VSDI response to a target element, termed "center", fell entirely within the imaged area.

250 The primary goal of the current study was to measure the spatial properties of the VSDI response  
251 amplitude (peaks of solid blue curve in Figure 1c) rather than the temporal dynamics. Because we are  
252 interested in subtle interactions, it was important to maximize our signal-to-noise ratio (SNR). The  
253 variability in the VSDI signal is dominated by low temporal frequencies. Therefore, to improve the SNR  
254 of our VSDI measurements, each one-second stimulus presentation consisted of 5 on/off cycles (Figure  
255 1c, gray bars). This improves the VSDI SNR by an order of magnitude (Chen et al., 2012). To estimate  
256 the peak amplitude, we assumed that each pulse, if presented alone, would produce a response that is  
257 well described by a scaled gamma distribution function (dashed curves). The simplest hypothesis is that  
258 responses to the individual pulses combine linearly. However, we found that the max of the individual  
259 responses in time (solid black curve) provide a slightly better description of the combined response.  
260 Therefore, the VSDI response amplitude was defined as the peak height of the best-fitting (in a least-  
261 squares sense) scaled gamma distribution function (i.e., the peak height of the dashed black curve in

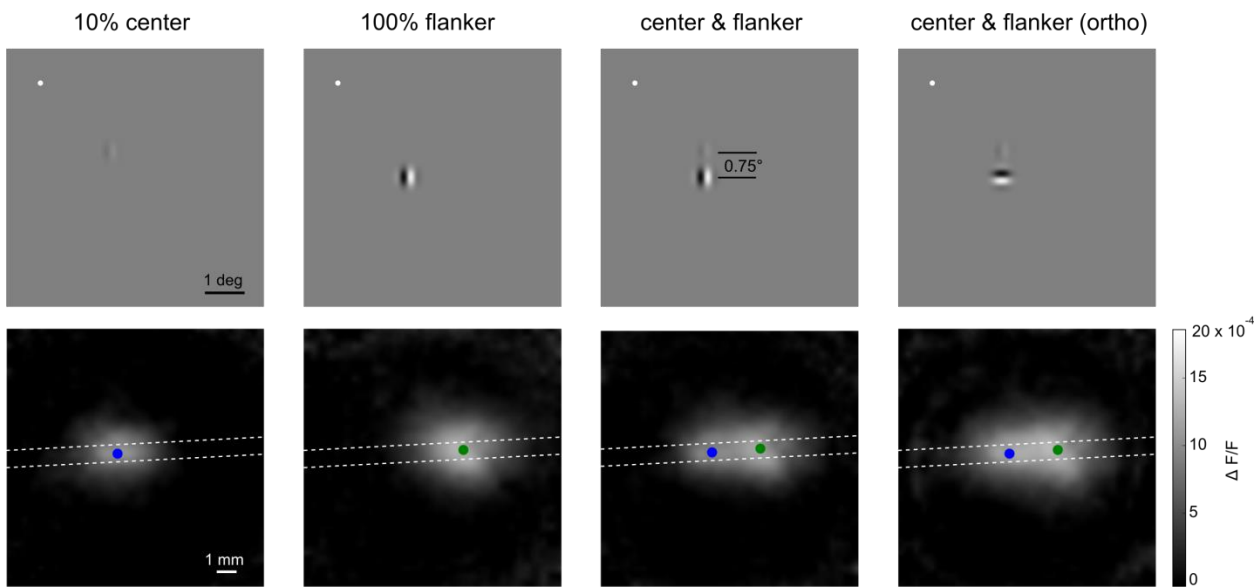
Figure 1c). Nonetheless, we found that the results described below are essentially the same using the amplitude of the gamma distribution function in the linear temporal model (data not shown).



**Figure 1.** Cortical retinotopy and temporal response profile in an example experiment. **a** Schematic illustration of the visual field with 1°x1° rectangular grid. The colored lines represent the approximate limits of visual space represented in our imaging windows. **b** Image of the cortical vasculature across a 10 × 10 mm region of V1 (Monkey 1, left hemisphere) with overlaid scale marker, landmarks, and approximate retinotopy for the rectangular grid shown in (a). **c** The time course of the stimulus presentation (with gray bars representing periods of stimulus presentation) and of the corresponding neural responses. Stimulus presentations consisted of repeated 60ms presentations of a Gabor pattern separated by 140ms presentations of a blank gray screen. The blue curves represent the average VSDI response in a 1x1 mm<sup>2</sup> centered on the peak spatial response to the 100% (solid) and 10% (dashed) contrast Gabor stimuli, as a function of time, while the dashed black curve represents the fitted response (see text) for a single 60 ms pulse of the 100% contrast stimulus. Response amplitudes were well described by a model in which individual pulse response functions were combined using a maximum rule (solid black curve).

## Population Responses to Single Gabor Stimuli

Consistent with our previous results (e.g., Chen et al., 2006; Michel et al., 2013; Palmer et al., 2012; Sit et al., 2009), single Gabor elements activated a localized ellipsoidal region, well described by a 2D Gaussian surface, that subtended several square millimeters of V1 (Figure 2, first and second columns). The response to the target was anisotropic, with the major axis of the response ellipsoid oriented parallel to the V1/V2 border (Figures 1b and 2;  $\sigma_{major} \approx 1.9$  mm;  $\sigma_{minor} \approx 1.2$  mm). Because the Gabor stimuli are small relative to the subthreshold receptive fields of V1 neurons at these eccentricities, the spatial extent of the activation across the cortical surface reflects the subthreshold CPI (Chen et al., 2012). Due to the membrane-potential-to-spikes nonlinearity, the spatial extent of the VSDI response is about twice as large as the spatial extent of the spiking cortical response (Chen et al., 2012). Responses were measured to several different stimulus contrasts. The response amplitude depended strongly on contrast; however, as in previous experiments (Chen et al., 2006), the spatial profile of the response was largely contrast invariant.



**Figure 2.** Visual stimulus configurations (top) and corresponding spatial response profiles (bottom) measured from V1 of Monkey 2 and averaged across 4 experiments. Response amplitudes ( $\Delta F/F$ ) were computed as described in Fig. 1c. The blue and green dots indicate the mean locations of peak of the 2-D Gaussians fit to the response profiles elicited by 10% contrast ‘center’ and 100% contrast ‘flanker’ Gabor patterns, respectively. The dashed white lines denote the boundaries of a 1 mm wide strip centered on the line passing through the center of these mean locations. The first and second columns from the left represent the center-only and flanker-only conditions, respectively, while the third and fourth columns represent conditions in which both elements were presented simultaneously. The forth column, labeled “center & flanker (ortho)”, represents the stimulus configuration and elicited response when the orientation of the high-contrast ‘flanker’ is orthogonal to that of the low-contrast ‘center’ element.

### ***Population Responses to Paired Gabor Stimuli***

Our primary goal was to characterize the population response to multiple visual elements. Previous single-unit studies in V1 reported that elements outside the classical receptive field can facilitate or suppress the responses to oriented stimuli in the center of the receptive field. When the contrast of the center element is low, collinear flanking elements that fall outside of the classical receptive field tend to facilitate the response to the center element (Kapadia et al., 1995; Polat et al., 1998). This has led to the hypothesis that this neurophysiological facilitation underlies some of the flanker facilitation effects reported in the psychophysical literature (Polat and Sagi, 1993; Kapadia et al., 1995). Therefore, we were particularly interested in measuring population responses to collinear stimulus configurations similar to those used in the psychophysical studies. The experimental stimulus conditions (Figure 2) consisted of: 1) a “center-only” condition, in which a low-contrast (10%) vertical target element was presented alone, 2) a “flanker-only” condition, in which a high-contrast (100%) vertical element, offset from the position of the center element, was presented alone, 3) a combined “center & flanker” condition in which the low-contrast center element and high-contrast flanker were presented

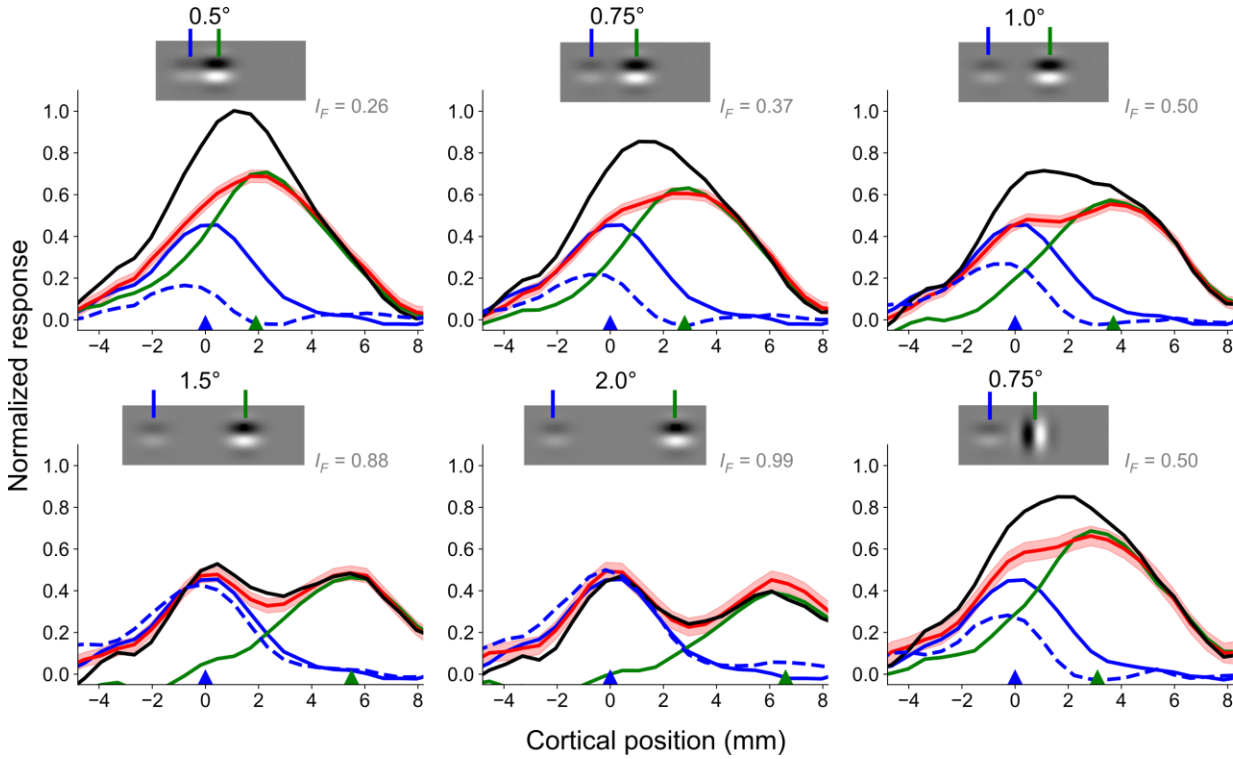




curves represent amplitudes of the VSDI responses to the center element presented alone, green curves to the flanker element presented alone, and red curves to the simultaneous presentation of both elements, for stimulus configurations having four inter-element distances (IEDs) and two center-flanker alignment conditions. The blue and green triangles at the bottom of each panel represent the peak response locations for the center and flanker elements, respectively, computed using 2-D Gaussians fit to the cortical responses (see Fig. 2). Black curves represent the responses expected under linear combination (summation) of ‘center’ and ‘flanker’ responses. Dashed blue curves represent the net response to the target in the combined condition, after subtracting the response to the flanker (i.e., the red curve minus the green curve); if the responses are additive, then the dashed blue curve must overlay the blue curve. The gray text insets indicate the computed facilitation index (see text), with  $I_F$  values smaller than 1 indicating sublinear combination.

To analyze the response amplitude at different cortical locations in V1, we defined a narrow 1-mm wide strip (Figure 2, dashed lines) around the line connecting the peaks of the spatial responses to center (blue dot) and flanker (green dot) elements. Within this strip, we divided the imaging pixels into small (~0.5 mm) bins according to their locations along the strip, averaging the response amplitudes within each bin. Example measurements from one monkey at five different positions of the flanker are shown in Figure 3. The response to the center element alone is shown in blue and is the same in all panels. The response to the flanker alone is shown in green and the combined response in red. Due to the spatial extent of the neural activity noted above, the flankers typically elicited substantial activity at the cortical site corresponding to the peak of the center stimulus (Figure 3, green curves). Our analysis focused on examining how the responses elicited by the flanker elements interacted with the response elicited by the center element. The black curves show the sum of the responses to the center alone and flanker alone. Note that the red curves are substantially below the black curves except at the largest separation, indicating strong subadditivity. Another way to visualize the degree of additivity is to subtract the response to the flanker alone from the response to the combined stimuli (dashed blue curve), which is equivalent to asking what is the response to the center in the presence of the flanker. If the responses to

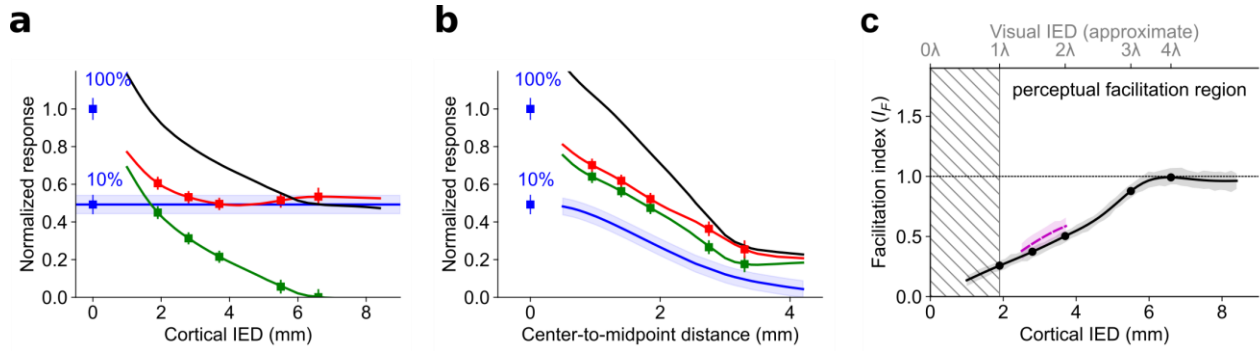
the center and flanker element were additive then the dashed blue curve would be superimposed on the solid blue curve. Figure 4 shows the combined measurements from all the experiments in all three monkeys (see Methods for details about how the measurements were combined). As can be seen, the pattern of results is quite similar to the example measurements in Figure 3.



**Figure 4.** Comparison of spatial response profiles across all conditions and experiments ( $N = 14$ ) in all three monkeys; see legend for Figure 3.

We carried out several different analyses to quantify the interactions between the center and flanker elements. First, we computed the response at the center location as function of the cortical separation between the center and the flanker, for center alone, flanker alone, and center plus flanker (Figure 5a). To do this, we averaged the data across all experiments after normalizing the responses in each experiment by the response to the 100% contrast center element presented alone. The response to the

center element at 10% contrast (blue horizontal curve) was about 40% of that to the center element at 100% contrast. The response at the center location to the flanker element alone was larger than that to the center element when the inter-element separation was less than 2.5 mm, and fell to zero at about 6 mm separation (green curve). The response to the combined stimulus was equal to the response to the flanker alone at small separations, and became equal to the response to the center alone at a separation of around 4 mm (red curve). At every separation where the flanker was still producing a significant response at the center location, the combined response was strongly sub-additive (compare red and black curves).



**Figure 5.** Summary of spatial response properties across all experiments. **a** Normalized average response amplitude in a  $1 \times 1$  mm cortical patch representing the location of the peak response to the center element (i.e., the blue dot in Fig. 2) as a function of the inter-element cortical distance between the center and flanker elements. As in Fig. 4, the blue curves represent the amplitude of the VSDI responses to the center element alone, the green curves represent the responses to the flanker alone, the red curves represent the observed responses to the combined (center and flanker) stimulus, and the black curves represent the responses expected under linear combination. Markers represent pooled responses computed at each of the five stimulus IEDs shown in Fig. 4. Shaded regions and error bars represent 95% confidence intervals for the mean response amplitude. **b** Same as **a** but for a cortical patch representing the midpoint between the peak responses to the center and flanker elements. **c** The value of the facilitation index  $I_F$  computed for the pooled spatial responses as a function of cortical inter-element distance (bottom axis) and as a function of the inter-element separation measured in wavelengths  $\lambda$  of the Gabor carrier (top axis). The solid black curve represents the facilitation index computed for collinear stimulus

configurations, while the dashed magenta curve represents the facilitation index computed for orthogonal stimulus configurations. The shaded areas represent 95% confidence intervals determined using a bootstrap procedure. The unhatched region on the right side of the plot represents the range of distances over which significant behavioral threshold facilitation has been demonstrated (e.g., Polat & Sagi, 1993).

Next, we used the same procedure to characterize the interactions at the midpoint between cortical locations of the peak responses to the center and the flanker (Fig. 5b). Note that in this case the cortical separation from the midpoint to the center of each stimulus is half the cortical separation between the elements. Again, the combined response is equal to the flanker-alone response at small inter-element separations and is strongly sub-additive at all inter-element separations out to about 3 mm from the midpoint, beyond which the combined response becomes fairly linear.

Finally, to summarize the interactions at all spatial locations along the line connecting the peak responses, we used a simple facilitation index. To compute this index we took the difference between in the response to center plus flanker and flanker alone (dashed blue curves in Figure 4) and then divided by the response to the center alone (solid blue curves in Figure 4). The value of the index was defined to be the average over a spatial strip measuring  $4 \times 1$  mm, centered on the peak response to target alone. Formally the index is defined by the following equation:

$$I_f = \frac{1}{n_C} \sum_{x \in \Omega_C} \frac{r_{C+F}(x) - r_F(x)}{r_C(x)} \quad (12)$$

where  $r_{C+F}(x)$  is the response to the center plus flanker,  $r_F(x)$  is the response to the flanker alone,  $r_C(x)$  is the response to the center alone,  $\Omega_C$  is the set of spatial locations over which the average is computed, and  $n_C$  is the number of points in the set of spatial locations. An index value greater than 1.0

indicates facilitation; an index value equal to 1.0 indicates additivity (independence); an index value less than 1.0 indicates sub-additivity. The facilitation index values are given in Figures 3 and 4, and are plotted for all separations between center and flanker in Figure 5c. Strong sub-additivity is observed when the flanker element is near the center element and approaches additivity when the flanker exceeds a distance of 6 mm. Facilitation was not observed at any separation. This pattern is broadly consistent with previous studies (e.g., Grinvald et al., 1994; Kinoshita et al., 2009; Meirovithz et al., 2010) that used different stimuli and recording techniques to examine lateral interactions in V1 population activity.

We next examined the responses when the flanker element was orthogonal to the center element. The upper right panel in Figure 3 and the lower right panel in Figure 4 show the results for the orthogonal condition. Clear subadditivity was also observed in the orthogonal conditions. Furthermore, the average facilitation index across all monkeys was slightly lower (more subadditive) for the collinear conditions than for the orthogonal conditions (see Figure 4).

### ***Population Gain-Control Model & Simulations***

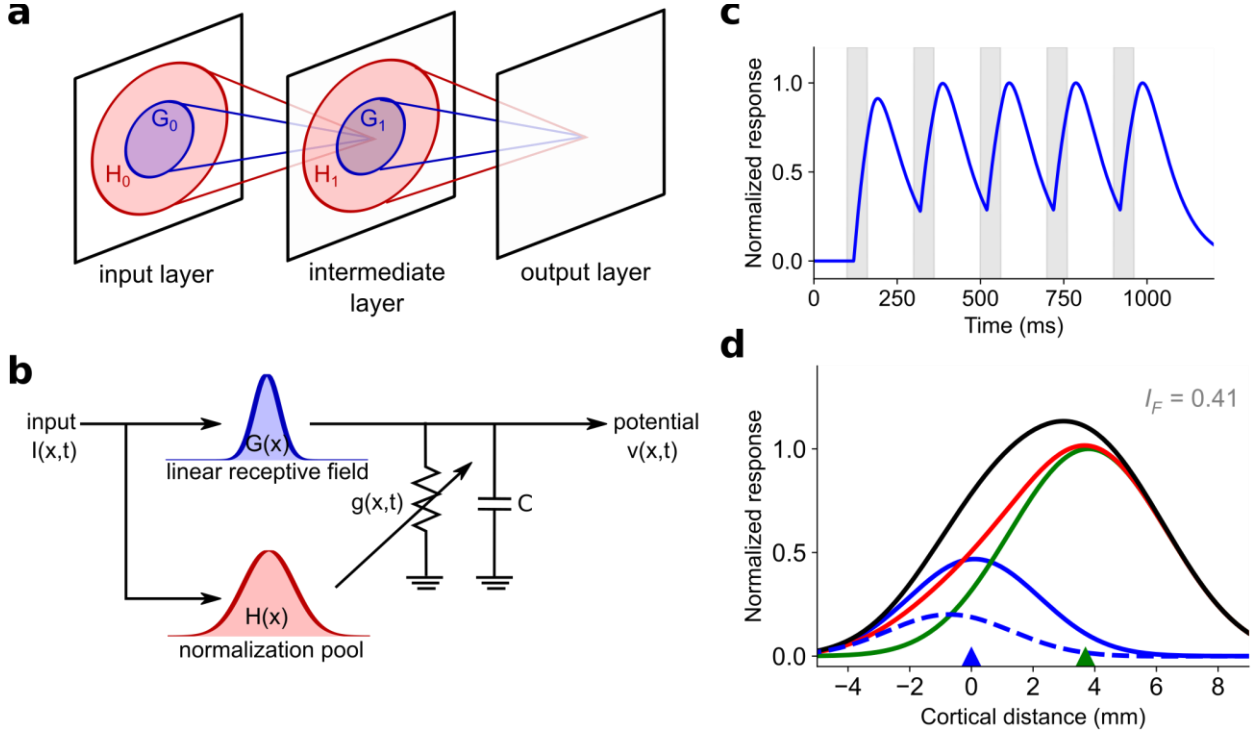
The primary goal of the present study was to use VSDI to begin characterizing the population responses in V1 to multiple visual elements. Our choice of small oriented elements was motivated in large part by psychophysical studies that have found strong facilitatory detection effects and contour-grouping effects for such stimuli. If the mechanisms underlying these effects are located in V1, then we should have observed facilitatory interactions for certain configurations of the elements in our experiments. Instead the interactions we observed were either additive or sub-additive, suggesting that the mechanisms underlying the facilitatory-detection and contour-grouping effects are primarily downstream of the membrane potential activity in V1 (however, see Discussion).

A stronger test of this hypothesis is to determine whether the multi-element interactions we measured can be accounted for by the well-known suppressive mechanisms that have been identified in V1.

In previous work, we found that VSDI responses to single element stimuli were well-predicted by a population gain control (PGC) model (Sit et al., 2009) based on the contrast gain-control mechanisms that have been identified in single unit studies (Albrecht and Geisler, 1991; Heeger, 1992; Carandini and Heeger, 1994; Carandini et al., 1997; Cavanaugh et al., 2002). In the PGC model, the gain of the response of a group of neurons at a given cortical location is controlled divisively by the pooled activity of a (potentially more spatially extended) population of neurons (the “normalization pool”). Thus, according to this model, a flanking stimulus that does not directly activate a group of V1 neurons responding to a central element, may nevertheless affect their response if it activates neurons in the normalization pool. Such an effect is expected to be suppressive or sub-additive, as flanking stimuli will reduce the gain of the response to the central element.

The model (Figure 6a,b) consists of an input layer representing the raw visual input, a second layer representing the local spatial summation and gain control arising in the retina, LGN, and the input layers of V1, and a third layer that represents the local spatial summation and gain control in the superficial layers of V1, where the VSDI responses are measured. The blue and red regions represent the spatial summation and gain-control (normalization) pools, respectively, for each location in the subsequent layer. As indicated in the figure, the normalization pool has a larger spatial extent than the summation pool, in agreement with the single unit literature (Cavanaugh et al., 2002). Each unit computes two weighted sums of the units in the projecting layer. One of these sums,  $G(x)$ , controls the input current, and the other,  $H(x)$ , controls the conductance, and thus the gain of the circuit. The output voltage of this simple RC circuit represents the unit's response. We note that this is a functional/computational model

that is not meant to represent any specific biophysical mechanism. More details of the model can be found in Sit et al. (2009).

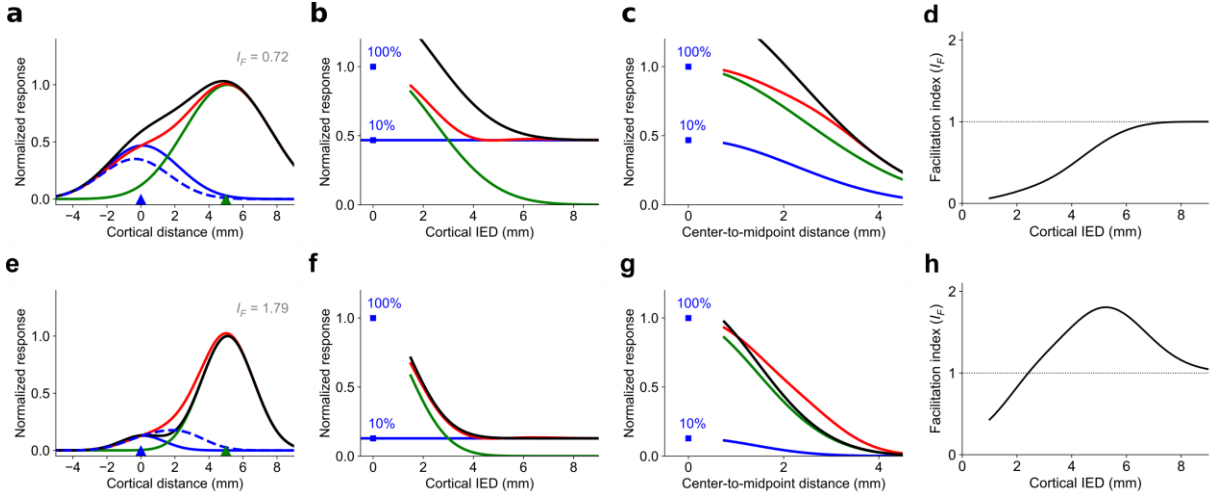


**Figure 6.** Population gain control (PGC) model and response properties. **a** The model (from Sit et al., 2009) consists of an input layer representing the raw visual input, an intermediate layer representing the nonlinearities arising in the retina, LGN, and the input layers of V1, and a third layer that represents the superficial layers of V1, where the VSDI responses are measured. The blue and red regions represent the receptive fields and normalization pools, respectively, of individual units in the subsequent layers. **b** The processing in a model unit (intermediate and output layers). Each unit computes two weighted sums ( $G(x)$  and  $H(x)$ ) of the units in the projecting layer that feed into a parallel RC circuit, with  $G(x)$  controlling the input current,  $H(x)$  controlling the conductance and thus the gain of the circuit, and the voltage across the capacitor representing the unit's response. (Panels **a** and **b** modified from Sit et al., 2009). **c** A sample of the PGC model's temporal response profile for the stimuli used in the current study (symbols as in Fig. 1c). **d** A sample of the PGC model's spatial response profile (cross section) for stimuli used in the current study. Here, the Gabor elements are spaced  $1^\circ$  apart at an assumed cortical magnification factor (CMF) of  $3.7 \text{ mm}/^\circ$  (symbols as in Fig. 4).



458 Figure 6c shows the PGC model's response to a stimulus consisting of a single element. As can be seen,  
459 the temporal dynamics predicted by the model are largely consistent with the observed dynamics  
460 (compare with Figure 1c). For example, the model's responses are also better described as the max of  
461 the individual responses in time rather than the sum of the responses. To generate predictions for the  
462 spatial responses to single and multiple elements, we applied the same method used to analyze the VSD  
463 responses. Specifically, the model's response amplitude was defined as the peak height of the best-  
464 fitting (minimum squared error) scaled gamma distribution function as in Figure 1c. The blue curve in  
465 Figure 6d shows the predicted response across space to the center element alone, the green curve the  
466 response to the flanker element alone at a distance of 1 deg. The red curve shows the predicted response  
467 to the sum of the two elements, and black curve shows the linear sum of the responses to the two  
468 elements. Again these predictions are generally consistent with our results (upper right panel in Figure  
469 4).

470 Figure 7a-c summarizes the predicted response for all separations of the center and flanker elements.  
471 Again the predicted results are generally consistent with the data (Figure 5). When the element  
472 separation in cortex is small (less than 4 mm) then the combined responses are strongly sub-additive and  
473 become more linear at larger separations. The gain-control in the PGC model is not orientation tuned  
474 and hence it also predicts the equally strong suppression for the conditions with parallel and orthogonal  
475 flanker (Figure 4). In sum, the results of the modeling are consistent with the hypothesis that the  
476 interactions we observed in membrane-potential responses are primarily due to overlapping receptive  
477 fields and contrast gain control. In the Discussion, we consider the potential implications for spike  
478 responses.



**Figure 7.** Spatial response properties for the population-gain-control (PGC) model of membrane potential activity, for comparison with the VSDI results presented in Fig. 5. **a** A cross section of the PGC model's spatial response profile for Gabor elements whose peak responses are spaced 5.0 mm apart (symbols as in Fig. 4). **e** A spatial response profile corresponding to the same stimulus configuration after the PGC responses have been passed through a spiking nonlinearity. **b,f** Normalized responses computed at the location of the center, and **c,g** at the midpoint between the center and flanker elements. **d,h** Facilitation index of the PGC model as a function of cortical inter-element separation, computed using the cross sections of the spatial response patterns. The top panels (**a-d**) represent simulated subthreshold responses, while the bottom panels (**e-h**) represent the corresponding responses following application of a spiking nonlinearity.

## Discussion

We used voltage sensitive dye (VSD) imaging to measure the spatiotemporal neural-population responses in a large region of primary visual cortex (V1) to pairs of collinear and orthogonally-oriented stimulus elements. The VSD responses are proportional to the real-time summed membrane potential responses in the upper cortical layers (i.e., the output layers that project to other cortical areas), and can be measured over the entire area activated by the center stimuli (see Figure 2), making them ideal for characterizing interactions at the whole-population level. Our primary finding is that nearby contour

elements combine in a sub-additive fashion (mutual suppression) and that distant elements combine in a more additive fashion (simple summation). We also found slightly less suppression when the flanker element was orthogonal to the test element, consistent with Cavanagh et al. (2002b). We found no evidence of super-additive interaction (facilitation). Indeed, the results as a whole were qualitatively predicted by a population contrast-gain-control model consistent with the contrast-gain-control (normalization) mechanisms that have been identified in single-unit studies of the retina, LGN and visual cortex. Thus, our results would seem most consistent with the hypothesis that most of the (presumably) facilitatory neural interactions that underlie behavioral contour detection and contour grouping performance occur downstream of primary visual cortex.

Nonetheless, VSDI measures membrane potentials rather than spiking activity, and it is the spiking activity in the upper cortical layers that is being transmitted to other cortical areas. Intracellular recording of cortical neurons shows that there is a nonlinear relationship between membrane potential and spike rate. Specifically, spike rate is approximately a power function of the membrane potential with an exponent that averages around 3.0 (Priebe and Ferster, 2008; Tan et al., 2014). A power exponent greater than 1.0 can lead to super-additivity. For example, if stimulus  $a$  and stimulus  $b$  alone produce a membrane-potential response of 2 (units arbitrary), then a power exponent of 3.0 will produce a spike response proportional to 8. If membrane potentials are additive, then the membrane-potential response to simultaneous presentation of both stimuli would be 4 ( $2+2 = 4$ ), and the spike response would be proportional to 48 ( $4^3 = 48$ ). This spike response is much larger than the sum of the individual spike responses, which would be proportional to 16 ( $8+8 = 16$ ). Cardin et al., (2010) have empirically demonstrated this phenomenon (i.e., sub-additive response combination in membrane potentials leading

to super-additive response combination in the spiking responses) in intracellular recordings of individual V1 neurons.

To assess the potential effect of the spiking nonlinearity, we applied a power exponent to the predicted population membrane-potential responses of the PGC model. However, directly applying the average exponent measured in intracellular single-unit recording to the predicted VSD responses is not justified because applying a power exponent to individual membrane potentials and summing (which would estimate the spiking population activity) is not algebraically equivalent to summing the membrane potentials and then applying a power exponent. To evaluate this issue we simulated a large population of neurons having a distribution of half-saturation contrasts (values of  $c_{50}$ ) similar to those measured in macaque V1 (Albrecht and Hamilton, 1982; Sclar et al., 1990). To simulate population spiking activity we applied a response exponent of 3.0 to each individual neuron's membrane potential response and summed across the population. In comparison, we first summed the membrane-potential responses of all the neurons and then applied a response exponent. We found that applying a response exponent of 2.7 to the summed membrane potential responses closely matched the simulated summed spiking activity. Thus, applying an exponent of 2.7 to the predicted population membrane potential responses should give us approximately the results for population spiking activity.

A summary of this analysis is shown in Figure 7e-h, which is analogous to the membrane potential predictions in Figure 7a-d. When the element separation in cortex is small (less than 2 mm) then the combined responses are sub-additive, but they become facilitatory at separations between 2 and 7 mm, and additive beyond that. As mentioned above, the gain-control in the PGC model is not orientation tuned and hence it also predicts the same suppression and facilitation for the parallel and orthogonal flanker (Figure 4). The predicted facilitatory and suppressive effects are weak in Figure 7e, which shows

the predicted spiking responses at the location of the center element. Thus, the PGC model predicts that on average it should be relatively difficult to observe facilitatory or suppressive effects in the spiking activity of neurons with RFs centered on a low-contrast element when the flanker is greater than 1.5 mm distant. Figure 7f suggests that facilitatory responses should be relatively easier to observe by recording from neurons that are between the center and flanker elements. Figure 7g suggests that for spacing between center and flanking elements of 2-6 mm there should be strong facilitation in total spiking response pooled over a 4 x 1 mm region centered on the 10% contrast element.

The analysis in Figure 7e-h makes the important point that an entirely local spiking nonlinearity can create facilitatory interactions in spiking activity from purely suppressive (or additive) interactions at the level of membrane potentials. Indeed, for every V1 neuron we would expect there to be some separation of the two elements that could produce some super additivity due to the spiking nonlinearity. Thus, our VSDI results and the PGC model are not necessarily inconsistent some of the facilitatory effects reported in the single-unit literature.

Polat & Sagi (1993; Fig. 3) report, for psychophysical detection experiments with co-linear Gabor elements of similar spatial frequency and bandwidth to those tested here (note that they tested a variety of spatial frequencies), that suppression (threshold elevation) is observed up to distances equal to approximately the spatial wavelength  $\lambda$  (1/ spatial frequency) of the elements, and that facilitation is observed from there up to more than  $8\lambda$ . This range of distances corresponds to a range of  $0.5^\circ$  to  $4^\circ$  of visual angle for the stimuli used in the current experiment, which extends well beyond the maximal cortical IED at which we predict facilitation of spiking population responses (i.e.,  $\sim 8$  mm; Fig. 7h). Further, they find that when the flanking high-contrast element is orthogonal to the test element there is little effect on threshold, whereas we find weaker subthreshold suppression (and therefore stronger

spiking facilitation) for the orthogonal flanker (Figs. 4 and 5c). Thus, their results are not very consistent with our VSDI results and with the predictions of the population spiking activity in Figure 7e-h.

It is also important to note, that predicted facilitation in mean spiking activity in Fig. 7g-h does not directly imply better detection performance (i.e., better signal-to-noise ratio). Whether one should expect better detection performance depends on the sources of noise. For example, if the dominant noise is prior to the spiking nonlinearity then the nonlinearity should have little effect on detection performance.

A final question to consider is how our results might be related to the mechanisms of contour grouping. A standard view of contour grouping is that (1) local pattern-detection mechanisms identify oriented contour elements, (2) local grouping mechanisms bind/associate nearby elements that are consistent with the statistical properties of natural contours, and (3) global grouping mechanisms form representations of extended contours. There is little doubt that the receptive field properties of neurons in V1 contribute to step (1), but it is not so clear that they contribute to step (2). A recent study showed clear grouping related population signal in V1 of monkeys performing a grouping task (Gilad et al., 2013). However, these grouping related signals were significantly delayed relative to the visual responses, suggesting that these signals could reflect post-grouping attentional effects. The facilitatory lateral effects on detection performance and in V1 neural responses occur primarily when one of the contour elements has low or near-threshold contrast (Polat and Sagi, 1993, 1994; Kapadia et al., 1995). On the other hand, perceptual contour grouping is typically measured when the elements belonging to a contour are of high and equal contrast (Field et al. 1993). Single unit studies suggest that under such circumstances lateral interactions are generally suppressive (Polat et al., 1998; Sceniak et al., 1999; Cavanaugh et al., 2002; Levitt and Lund, 2002). It is still possible that there is a specialized subset of V1 neurons that contribute

to contour grouping or that the elongated RFs of V1 neurons contribute to local contour grouping (De Valois et al., 1982; Webster and De Valois, 1985; Ringach, 2002; Michel et al., 2013), but it seems likely that local and global contour grouping occur primarily in later cortical areas.

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